

A NEW NONLOCAL NONLINEAR DIFFUSION EQUATION: THE ONE-DIMENSIONAL CASE

G. ALETTI , A. BENFENATI  and G. NALDI  

(Received 11 December 2021; accepted 11 February 2022; first published online 5 May 2022)

Abstract

We prove a result on the existence and uniqueness of the solution of a new feature-preserving nonlinear nonlocal diffusion equation for signal denoising for the one-dimensional case. The partial differential equation is based on a novel diffusivity coefficient that uses a nonlocal automatically detected parameter related to the local bounded variation and the local oscillating pattern of the noisy input signal.

2020 *Mathematics subject classification*: primary 35K59; secondary 35K20.

Keywords and phrases: nonlocal diffusion equation, fixed point method, signal denoising.

1. Introduction

Nonlinear partial differential equations (PDEs) can be used in the analysis and processing of digital images or image sequences, for example, to extract features and shapes or to filter out the noise to produce higher quality images (see, for example, [3, 4, 14, 15] and the references therein). Arguably, the main application of PDE-based methods in this field is the smoothing and restoration of images. From the mathematical point of view, the input (grey scale) image can be modelled by a real function $u_0(x)$, $u_0 : \Omega \rightarrow \mathbb{R}$, where $\Omega \subset \mathbb{R}^d$ represents the spatial domain. Typically, this domain Ω is rectangular and $d = 1, 2$ or 3 . The function u_0 is considered as initial data for a suitable evolution equation with some kind of boundary conditions. The simplest (and oldest) PDE method for smoothing images is to apply a linear diffusion process: the starting point is the simple observation that the so-called Gauss function is related to the fundamental solution of the linear diffusion (heat) equation.

The flow produced by the linear diffusion equation spreads the information equally in all directions. Although this property is good for a local noise reduction in the case of additive noise, this filtering operation also destroys the image content such as the boundaries of the objects and the subregions present in the image. This means that the

The three authors are members of the Italian Group GNCS of the Italian Institute ‘Istituto Nazionale di Alta Matematica’ and of the ADAMSS Center of the Università degli Studi di Milano (Italy).

© The Author(s), 2022. Published by Cambridge University Press on behalf of Australian Mathematical Publishing Association Inc. This is an Open Access article, distributed under the terms of the Creative Commons Attribution licence (<https://creativecommons.org/licenses/by/4.0/>), which permits unrestricted re-use, distribution, and reproduction in any medium, provided the original work is properly cited.

Gaussian smoothing not only smooths noise, but also blurs important features in the signal.

Recently, a new anisotropic diffusion model was introduced in [11] to analyse experimental signals in neuroscience: the diffusivity coefficient uses a nonlocal parameter related to the local bounded variation and the local oscillating pattern of the noisy input signal. In [2], the model was extended to the multidimensional case with an analysis for the existence of the solution in the two-dimensional case (images) and the introduction of a suitable numerical scheme. In this note, we focus on the one-dimensional case providing a complete analysis of the nonlocal diffusion equation, including the uniqueness that was an open problem.

2. A one-dimensional nonlocal nonlinear model

There is a vast literature concerning nonlinear anisotropic diffusions with applications to image processing, which dates back to the seminal paper by Perona and Malik [12], who considered a discrete version of the problem

$$\begin{cases} \frac{\partial u}{\partial t} - \nabla \cdot (g(|\nabla u|)\nabla u) = 0 & \text{in } \Omega_T = (0, T) \times \Omega, \\ u(x, 0) = u_0(x) & \text{on } \Omega, \\ \frac{\partial u}{\partial \vec{n}}(x, t) = 0 & \text{on } \Gamma \times (0, T), \end{cases} \quad (2.1)$$

where $\Gamma = \partial\Omega$, the image domain $\Omega \subset \mathbb{R}^2$ is an open regular set (typically a rectangle), \vec{n} denotes the unit outer normal to its boundary Γ , $\nabla \cdot$ is the divergence operator, and $u(x, t)$ denotes the (scalar) image analysed at time (scale) t and point x . The initial condition $u_0(x)$ is, as in the linear case, the original image. To reduce smoothing at the edges, the diffusivity g is chosen as a decreasing function of the ‘edge detector’ $|\nabla u|$. Here, we introduce a nonlocal diffusive coefficient that considers the ‘monotonicity’ of the signal. In other words, a high modulus of the gradient may lead to a small diffusion if the function is also locally monotone. At the same time, we want to reduce the noise present, as in the case of linear diffusion. We focus on the one-dimensional case, more precisely, where $u : [a, b] \rightarrow \mathbb{R}$ is a real function defined on a bounded interval $[a, b]$, and on a subinterval $[c, d] \subset [a, b]$. We define the *local variation* $LV_{[c,d]}(u)$ of u on the interval $[c, d]$ by

$$LV_{[c,d]}(u) = |u(d) - u(c)|.$$

We also define the *total local variation* $TV_{[c,d]}(u)$ of u on the interval $[c, d]$ by

$$TV_{[c,d]}(u) = \sup_{\mathcal{P}} \sum_{i=0}^{n_P-1} |u(x_{i+1}) - u(x_i)|$$

where $\mathcal{P} = \{P = \{x_0, \dots, x_{n_P}\} \mid P \text{ is a partition of } [c, d]\}$ is the set of all possible finite partitions of the interval $[c, d]$.

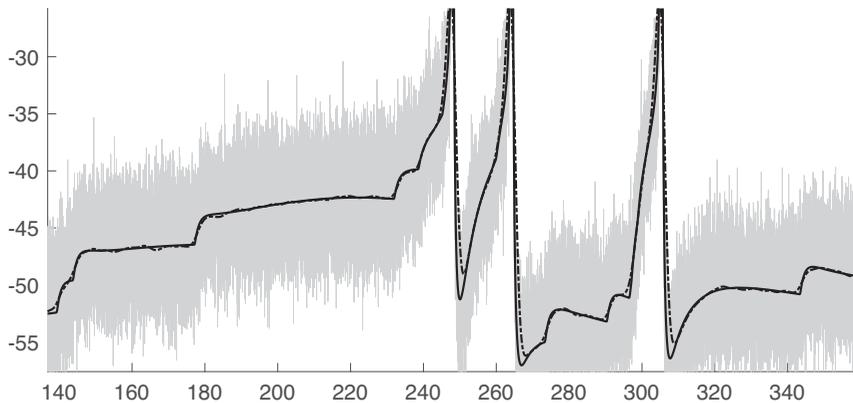


FIGURE 1. An illustrative example of signal denoising using the new nonlocal and nonlinear diffusion equation (2.2) with data from [1]. Solid line, original signal; grey line, signal with noise; dotted line, reconstructed signal.

Let $\varepsilon \in \mathbb{R}^+$, $\varepsilon \ll 1$, $\varepsilon > 0$ and let $\delta \in \mathbb{R}^+$. We define the ratio,

$$R_{\delta,u} = \frac{\varepsilon + LV_{[x-\delta,x+\delta]}(u)}{\varepsilon + TV_{[x-\delta,x+\delta]}(u)}.$$

If the parameter δ is chosen appropriately, we can distinguish between oscillations caused by noise contained in a range of amplitude δ . As in the Perona–Malik model given by (2.1), we adapt the diffusivity coefficient by using the above ratio $R_{\delta,u}$. For small values of the latter, we have to reduce the noise, while for values close to 1, the upper bound of $R_{\delta,u}$, we have to preserve the signal variation (as the edges in the image). The resulting diffusivity coefficient $g(R_{\delta,u})$ becomes nonlocal. We assume that $g : [0, +\infty) \rightarrow \mathbb{R}$ is a positive, nonincreasing, Lipschitz continuous function such that $g(0) = 1$ and $g(1) = \alpha > 0$. In the following, we assume that the parameter ε ($0 < \varepsilon \ll 1$) is fixed. In Figure 1, we show an illustrative example of a denoised signal using our nonlocal and nonlinear diffusion filter. In particular, we have numerically simulated (2.2) by adopting a semi-implicit method based on central finite differences (see [2]) and with the following numeric values of the parameters (see also (2.3)):

$$g(s) = \begin{cases} 1 & \text{if } s = 0, \\ 1 - s^2 e^{-3.315/(s/\lambda)^8} & \text{if } s \neq 0, \end{cases} \quad \lambda = 4, \quad \varepsilon = 10^{-3}, \quad \delta = 0.075,$$

and the time domain $t \in [0, 0.6]$ and space domain $x \in [0, 255]$. The signal in Figure 1 was obtained from a simulation of a biophysical model of a neuron with an additive Gaussian noise (mean equal to 0 and variance equal to 3) (see [1] for more details). The MATLAB code and the details are available from the authors.

In the following, $I = (a, b) \subset \mathbb{R}$ denotes a bounded open interval and $H^k(I)$, $k \in \mathbb{N}$, the Sobolev space of all functions u defined in I such that u and its distributional derivatives of order $1, \dots, k$ all belong to $L^2(I)$. Let D^s denote the distributional

derivative. Then $H^k(I)$ is a Hilbert space for the norm

$$\|u\|_k = \|u\|_{H^k} = \left(\sum_{|s| \leq k} \int_I |D^s u(x)|^2 dx \right)^{1/2}, \quad \|u\|_0 = \|u\|_{L^2}.$$

Let $L^p(0, T; H^k(I))$ be the set of all functions u , such that, for almost every t in $(0, T)$ with $T > 0$, $u(t)$ belongs to $H^k(I)$. Then $L^p(0, T; H^k(I))$ is a normed space for the norm

$$\|u\|_{L^p(0, T; H^k(I))} = \left(\int_0^T \|u\|_k^p dt \right)^{1/p},$$

where $p \geq 1$ and $k \in \mathbb{N}$. Finally, we denote by (\cdot, \cdot) the scalar product in $L^2(I)$.

We now establish our existence result. As initial conditions, we take the original signal u_0 but with some regularisation obtained with a standard smoothing filter, for example, a Gaussian filter, and we assume homogeneous Neumann conditions at the boundary.

THEOREM 2.1 (Existence). *Let $u_0 \in H^1(I)$ and $T > 0$, $\delta > 0$. Then there exists $u \in L^2(0, T; H^1(I)) \cap C^0([0, T]; L^2(I))$, satisfying $u(x, 0) = u_0(x)$ on I , $\partial u / \partial x = 0$ at $x = a, b$, and*

$$\frac{\partial u}{\partial t} - \frac{\partial}{\partial x} \left(g(R_{\delta, u}) \frac{\partial u}{\partial x} \right) = 0, \tag{2.2}$$

on $(0, T] \times I$ in the distributional sense.

PROOF. We show the existence of a weak solution of (2.2) by a classical fixed point theorem of Schauder (see, for example, [7, Theorem 2.2]). We introduce the space

$$V(0, T) = \left\{ v \in L^2(0, T; H^1(I)), \frac{dv}{dt} \in L^2(0, T; (H^1(I))') \right\}.$$

The space $V(0, T)$ is a Hilbert space with the graph norm. Let v be a function in $V(0, T) \cap L^\infty(0, T; L^2(I))$ such that

$$\|v\|_{L^\infty(0, T; L^2(I))} \leq \|u_0\|_{L^2(I)}.$$

We consider the following variational problem (P_v) :

$$\left\langle \frac{\partial u}{\partial t}(t), w \right\rangle + \int_I g(R_{\delta, v}) \frac{\partial u(t)}{\partial x} \frac{\partial w}{\partial x} dx = 0 \quad \text{for all } w \in H^1(I) \text{ (a.e.) in } [0, T]$$

$$u(0) \in H^1(I).$$

Here $\langle \cdot, \cdot \rangle$ represents the duality product. A function $u \in H^1(I)$ has locally bounded variation (see, for example, [10, Theorem 5.1]) and, moreover, is equal almost everywhere (a.e.) to an absolutely continuous function and u' exists a.e. and belongs

to $L^2(I)$. The term $R_{\delta,v}$ can be represented as

$$R_{\delta,v} = \frac{\varepsilon + \left| \int_{x-\delta}^{x+\delta} u'(s) ds \right|}{\varepsilon + \int_{x-\delta}^{x+\delta} |u'(s)| ds} \quad (2.3)$$

and $0 < R_{\delta,v} \leq 1$. So, $g(R_{\delta,v}) \geq \alpha > 0$.

Using classical results about parabolic equations (see, for example, [8, Theorem 10.1] and [9, Theorem 7.3]), the problem (P_v) has a unique solution $U(v)$ in $V(0, T)$. We can deduce the following estimates:

$$\begin{aligned} \|U(v)\|_{L^\infty(0,T;L^2(I))} &\leq \|u_0\|_{L^2(I)}, \\ \|U(v)\|_{L^2(0,T;H^1(I))} &\leq C_1, \\ \|U(v)\|_{L^2(0,T;(H^1(I))')} &\leq C_2, \end{aligned} \quad (2.4)$$

for suitable constants C_1 and C_2 depending only on u_0 , T and the Lipschitz constant of the function g . We introduce the subset V_0 of $V(0, T)$ defined by functions $v \in V(0, T)$ such that these estimates are satisfied and $v(0) = u_0$. Then U is a mapping from V_0 to V_0 . Moreover, V_0 is a nonempty, convex and weakly compact subset of $V(0, T)$.

To use the Schauder theorem, we have to prove that the mapping $v \rightarrow U(v)$ is weakly continuous from V_0 to V_0 . Then, since $V(0, T)$ is contained in $L^2(0, T; L^2(I))$ with compact inclusion, this yields the existence of $u \in V_0$ such that $u = U(u)$.

Let (v_j) be a sequence in V_0 which converges weakly to $v \in V_0$ and $u_j = U(v_j)$. From the classical theorems of compact inclusion (see, for example, [8, Theorem 9.16]), up to sub-sequences,

$$\begin{aligned} u_j &\rightarrow u \quad \text{weakly in } L^2(0, T; H^1(I)), \\ \frac{du_j}{dt} &\rightarrow \frac{du}{dt} \quad \text{weakly in } L^2(0, T; (H^1(I))'), \\ \frac{\partial u_j}{\partial x} &\rightarrow \frac{\partial u}{\partial x} \quad \text{weakly in } L^2(0, T; L^2(I)). \end{aligned}$$

Moreover, $u_j \rightarrow u$ in $L^2(0, T; L^2(I))$ and a.e. on $I \times (0, T)$ and $u_j(0) \rightarrow u(0)$ in $(H^1(I))'$. For the (v_j) , from (2.4), there is a subsequence such that $v_j \rightarrow v$ in $L^2(0, T; L^2(I))$ and, from the Rellich–Kodrachov theorem (see, for example, [9, Theorem 5.1], and (2.3)), $g(R_{\delta,v_j}) \rightarrow g(R_{\delta,v})$ in $L^2(0, T; L^2(I))$. By the uniqueness of the solution of (P_v) , the whole sequence $u_j = U(v_j)$ converges weakly in $V(0, T)$. Thus, the mapping U is weakly continuous from V_0 into V_0 and we can apply the Schauder theorem. \square

REMARK 2.2. A similar proof could be carried through in a more general case by considering a different measure of local variation, for example, using the absolute value of the difference between the maximum and minimum value in subintervals of length 2δ .

Under the hypotheses of Theorem 2.1, we have the following uniqueness result.

THEOREM 2.3 (uniqueness). *The solution $u \in L^2(0, T; H^1(I)) \cap C^0([0, T]; L^2(I))$ of (2.2), with $u(0) \in H^1(I)$ and homogeneous Neumann conditions, is unique.*

PROOF. Let \bar{u} and \hat{u} be two solutions of (2.2) and let $u = \bar{u} - \hat{u}$. Then for almost all t in $[0, T]$,

$$\frac{d\bar{u}}{dt} - \frac{\partial}{\partial x} \left(g(R_{\delta, \bar{u}}) \frac{\partial \bar{u}}{\partial x} \right) = 0, \quad \bar{u}(0) = u_0, \tag{2.5}$$

$$\frac{d\hat{u}}{dt} - \frac{\partial}{\partial x} \left(g(R_{\delta, \hat{u}}) \frac{\partial \hat{u}}{\partial x} \right) = 0, \quad \hat{u}(0) = u_0. \tag{2.6}$$

By subtracting (2.6) from (2.5),

$$\frac{d(\bar{u} - \hat{u})}{dt} - \frac{\partial}{\partial x} \left(g(R_{\delta, \bar{u}}) \frac{\partial \bar{u}}{\partial x} \right) + \frac{\partial}{\partial x} \left(g(R_{\delta, \hat{u}}) \frac{\partial \hat{u}}{\partial x} \right) = 0.$$

Adding and subtracting the quantity $\partial_x(g(R_{\delta, \bar{u}})\partial_x\hat{u})$, we can rewrite the equation as

$$\frac{du}{dt} - \frac{\partial}{\partial x} \left(g(R_{\delta, \bar{u}}) \frac{\partial u}{\partial x} \right) = \frac{\partial}{\partial x} \left([g(R_{\delta, \bar{u}}) - g(R_{\delta, \hat{u}})] \frac{\partial \hat{u}}{\partial x} \right). \tag{2.7}$$

Multiplying (2.7) by $u = (\bar{u} - \hat{u})$, integrating on the interval I , using the properties of the function g and the lower bound $g(1) = \alpha > 0$ and the estimates (2.4), we obtain

$$\frac{1}{2} \frac{d}{dt} \|u(t)\|_{L^2(I)}^2 + \alpha \left\| \frac{\partial}{\partial x} u(t) \right\|_{L^2(I)}^2 \leq C \|u(t)\|_{L^2(I)} \left\| \frac{\partial}{\partial x} \hat{u}(t) \right\|_{L^2(I)} \left\| \frac{\partial}{\partial x} u(t) \right\|_{L^2(I)},$$

for a suitable constant C . The term on the right-hand side can be estimated, using Young’s inequality, by

$$\frac{2}{\alpha} C^2 \|u(t)\|_{L^2(I)}^2 \left\| \frac{\partial}{\partial x} \hat{u}(t) \right\|_{L^2(I)}^2 + \frac{\alpha}{2} \left\| \frac{\partial}{\partial x} u(t) \right\|_{L^2(I)}^2.$$

Subtracting the term $(\alpha/2) \|(\partial/\partial x)u(t)\|_{L^2(I)}^2$ on both sides and using the *a priori* estimates (2.4), we get the inequality

$$\frac{1}{2} \frac{d}{dt} \|u(t)\|_{L^2(I)}^2 + \frac{\alpha}{2} \left\| \frac{\partial}{\partial x} u(t) \right\|_{L^2(I)}^2 \leq C^* \|u(t)\|_{L^2(I)}^2, \tag{2.8}$$

where $C^* = 2C^2C_1/\alpha$. Since $\bar{u}(0) = \hat{u}(0) = u_0$, by the inequality (2.8) and Gronwall’s lemma (see, for example, [13, Theorem 1.8]), we obtain the uniqueness of the solution. □

REMARK 2.4. Similar nonlocal equations could be obtained as diffusive limits from different kinetic microscale descriptions of the interactions of active particles (see, for example, [5, 6]).

References

- [1] G. Aletti, D. Lonardonì, G. Naldi and T. Nieuw, ‘From dynamics to links: a sparse reconstruction of the topology of a neural network’, *Commun. Appl. Ind. Math.* **10**(2) (2019), 2–11.

- [2] G. Aletti, M. Moroni and G. Naldi, 'A new nonlocal nonlinear diffusion equation for data analysis', *Acta Appl. Math.* **168**(1) (2020), 109–135.
- [3] I. Alvarez, F. Guichard, P.-L. Lions and J.-M. Morel, 'Axioms and fundamental equations of image processing', *Arch. Ration. Mech. Anal.* **123** (1993), 199–257.
- [4] S. Angenent, E. Pichon and A. Tannenbaum, 'Mathematical methods in medical image processing', *Bull. Amer. Math. Soc. (N.S.)* **43** (2006), 365–396.
- [5] A. Benfenati and V. Coscia, 'Nonlinear microscale interactions in the kinetic theory of active particles', *Appl. Math. Lett.* **26**(10) (2013), 979–983.
- [6] A. Benfenati and V. Coscia, 'Modeling opinion formation in the kinetic theory of active particles I: spontaneous trend', *Ann. Univ. Ferrara* **60** (2014), 35–53.
- [7] F. F. Bonsall, *Lectures on Some Fixed Point Theorems of Functional Analysis* (Tata Institute of Fundamental Research, Bombay, 1962).
- [8] H. Brezis, *Functional Analysis, Sobolev Spaces and Partial Differential Equations*, Universitext (Springer, New York, 2011).
- [9] L. C. Evans, *Partial Differential Equations*, Graduate Studies in Mathematics, 19 (American Mathematical Society, Providence, RI, 1998).
- [10] L. C. Evans and R. F. Gariepy, *Measure Theory and Fine Properties of Functions*, Textbooks in Mathematics (CRC Press, Boca Raton, 2015).
- [11] G. Palazzolo, M. Moroni, A. Soloperto, G. Aletti, G. Naldi, M. Vassalli, T. Nieuw and F. Difato, 'Fast wide-volume functional imaging of engineered in vitro brain tissues', *Sci. Rep.* **7** (2017), Article no. 8499, 20 pages.
- [12] P. Perona and J. Malik, 'Scale-space and edge detection using anisotropic diffusion', *IEEE Trans. Pattern Anal. Mach. Intell.* **12** (1990), 629–639.
- [13] L. C. Piccinini, G. Stampacchia and G. Vidossich, *Ordinary Differential Equations in R^n : Problems and Methods*, Applied Mathematical Sciences, 39 (Springer-Verlag, New York, 1984).
- [14] G. Sapiro, *Geometric Partial Differential Equations and Image Analysis* (Cambridge University Press, Cambridge, 2006).
- [15] J. Weickert, *Anisotropic Diffusion in Image Processing*, ECMI Series (B. G. Teubner, Stuttgart, 1998).

G. ALETTI, Environmental Science and Policy Department,
Università degli Studi di Milano, 20133 Milan, Italy
e-mail: giacomo.aletti@unimi.it

A. BENFENATI, Environmental Science and Policy Department,
Università degli Studi di Milano, 20133 Milan, Italy
e-mail: alessandro.benfenati@unimi.it

G. NALDI, Advanced Applied Mathematical and Statistical Sciences Center,
Università degli Studi di Milano, 20133 Milan, Italy
e-mail: giovanni.naldi@unimi.it